

mechanical force balance

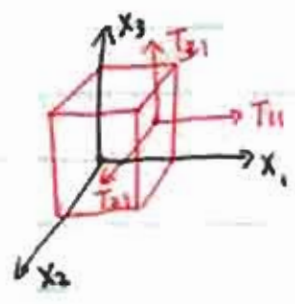
$F = ma \Rightarrow$ useful balance eqn for biological fluid situations, incompressible fluid, linear stress-strain, Newtonian viscosity flow/law.

Navier-Stokes Eqn

fluid velocity $\rho \frac{D\mathbf{v}}{Dt} = \rho \mathbf{g} + \rho_0 \mathbf{E} - \nabla p + \mu \nabla^2 \mathbf{v}$

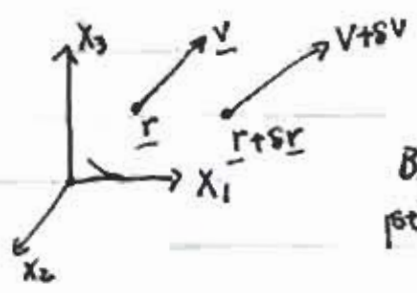
fluid density ρ gravity $\rho \mathbf{g}$ electric field forces $\rho_0 \mathbf{E}$ pressure gradient $-\nabla p$ viscous stress $\mu \nabla^2 \mathbf{v}$

$\nabla \cdot \mathbf{I}$ arise from surface force tensor, \mathbf{I}



$$\mathbf{I} = \begin{bmatrix} T_{11} & T_{12} & T_{13} \\ T_{21} & T_{22} & T_{23} \\ T_{31} & T_{32} & T_{33} \end{bmatrix}$$

T_{ij} = force per area in i th direction on surface whose normal is in j direction



unit vector
let $\mathbf{v} = v_1 \mathbf{x}_1 + v_2 \mathbf{x}_2 + v_3 \mathbf{x}_3$

By Taylor Series expansion, truncating @ 1st order $\delta \mathbf{v} = \mathbf{D} \delta \mathbf{r} + O(\delta r^2)$
fluid deformation

$$\delta \mathbf{v} = \begin{bmatrix} \delta v_1 \\ \delta v_2 \\ \delta v_3 \end{bmatrix} \quad \delta \mathbf{r} = \begin{bmatrix} \delta x_1 \\ \delta x_2 \\ \delta x_3 \end{bmatrix}$$

$$\mathbf{D} = \begin{bmatrix} \frac{\partial v_1}{\partial x_1} & \frac{\partial v_1}{\partial x_2} & \frac{\partial v_1}{\partial x_3} \\ \frac{\partial v_2}{\partial x_1} & \frac{\partial v_2}{\partial x_2} & \frac{\partial v_2}{\partial x_3} \\ \frac{\partial v_3}{\partial x_1} & \frac{\partial v_3}{\partial x_2} & \frac{\partial v_3}{\partial x_3} \end{bmatrix}$$

$$\delta \mathbf{v} = \mathbf{D} \delta \mathbf{r} \quad \text{or} \quad \delta v_i = \frac{\partial v_i}{\partial x_j} \delta x_j$$

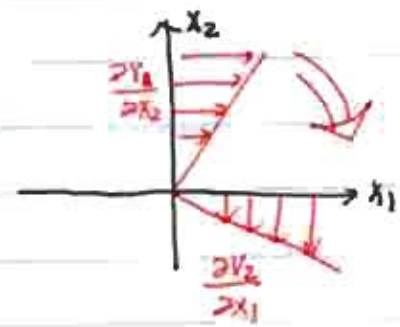
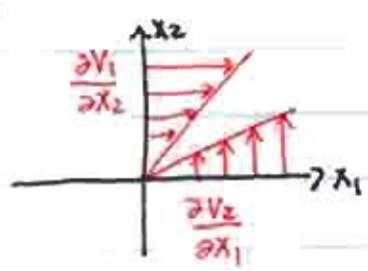
"Einstein Notation for summation"

Decompose \underline{D} into symmetric and anti-symmetric parts

$$\underline{D} = \underline{e} + \underline{\eta}$$

$$e_{ij} = \frac{1}{2} \left(\frac{\partial v_i}{\partial x_j} + \frac{\partial v_j}{\partial x_i} \right) \text{ shear}$$

$$\eta_{ij} = \frac{1}{2} \left(\frac{\partial v_i}{\partial x_j} - \frac{\partial v_j}{\partial x_i} \right) \text{ rotation}$$



Newtonian fluid:

$$\underline{T} = \underline{C} \underline{\epsilon}$$

Surface stress tensor \uparrow \underline{T}
 Strain rate tensor \uparrow $\underline{\epsilon}$
 $3 \times 3 \times 3 \times 3 = 81$ coefficients

In an isotropic fluid, δI reduces to 2. So,

$$T_{ij} = 2\mu e_{ij} + (\lambda - \frac{2}{3}\mu) \delta_{ij} e_{kk}$$

\uparrow \uparrow \uparrow
 \underline{T} (3x3) 1st Lamé coefficient (viscosity) 2nd Lamé coefficient
 Kronecker delta

In an incompressible fluid (essentially all of biology)

$$T_{ij} = 2\mu e_{ij} - p \delta_{ij}$$

\uparrow \uparrow \uparrow
 \underline{T} viscosity fluid strain rate pressure

$$\delta_{ij} = \begin{cases} 0 & \text{if } i \neq j \\ 1 & \text{if } i = j \end{cases}$$

Scaling argument:

let $\underline{w} = \frac{\underline{v}}{v_{max}}$, $\xi = \frac{r}{L}$, $\tau = \frac{t}{(L/v_{max})}$

\uparrow \uparrow
 presume

Reynold's Number

$$\frac{\rho v_{max} L}{\mu \nabla^2 v} = \left(\frac{\rho v_{max} L}{\mu} \right) \frac{Dv}{Dt} \frac{1}{\nabla^2 w}$$

In most (though not all), biological fluid systems:

$$Re \ll 1$$

Example - bacterial motility in water



$$L \sim 1 \mu m, V \sim 10 \mu m/sec$$

$$\rho \sim 1 g/ml$$

$$\mu \sim 1 cp = 10^{-3} kg/m \cdot sec$$

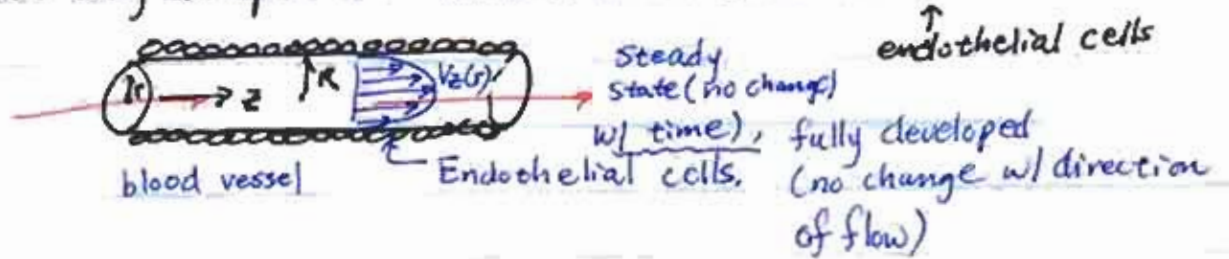
$Re = 10^{-5} \Rightarrow$ good approximation in most biology problems is

$$\rho \frac{Dv}{Dt} \rightarrow 0 \Rightarrow 0 = \rho g + \rho_e E$$

$$-\nabla p + \mu \nabla^2 v$$

Stokes Eqn

Quick + easy example #1: What is shear force on ECs?



$$\text{Stokes Eqn: } 0 = \frac{\mu}{r} \frac{\partial}{\partial r} \left(r \frac{\partial v_z}{\partial r} \right) - \frac{\partial p}{\partial z}$$

pressure drop in axial direction

Non-Newtonian behavior of blood due to high protein conc. & cell densities - exacerbated in domains a cell dimension.

$$v_z(r) = \underbrace{2\bar{v}}_{\text{mean velocity}} \left(1 - \left[\frac{r}{R} \right]^2 \right) = \frac{\int_0^R v_z(r) 2\pi r dr}{\int_0^R 2\pi r dr} = \frac{R^2}{8\mu} \left(-\frac{dp}{dz} \right)$$

Volumetric flow rate $Q = \bar{V} \cdot \pi R^2 = \frac{\pi R^4}{8\mu} \left(-\frac{dp}{dz}\right)$

viscous fluid stress on vessel wall (ECs):

$$\tau_{\theta r} = -\mu \left. \frac{dv_z}{dr} \right|_{r=R} = -\frac{4\mu \bar{V}}{R}$$

Example numbers -

Venule $R \sim 20 \mu\text{m}$
 $V \sim 200 \mu\text{m/s}$
 $\mu \sim 3 \text{ cp} (-3 \times 10^{-3} \text{ kg/m}\cdot\text{sec})$
 ↑
 blood, thicker than water

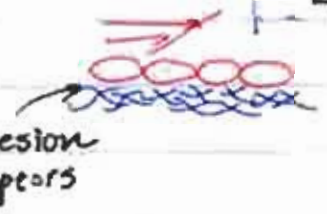
From Example 2.

Overall force on bacterium

$$F = -2\pi R^2 \int_0^\pi [p(R, \theta) \cos \theta + \tau_{\theta r}(R, \theta) \sin \theta] d\theta$$

↑ ↑
"drag" (shear)
 $2\pi \mu V_{\text{max}} R$ $4\pi \mu V_{\text{max}} R$
 (pressure) (shear)
 $= 6\pi \mu V_{\text{max}} R$

$\tau_{\theta r} \sim 0.1 \text{ N/m}^2, 0.1 \mu\text{N}/\mu\text{m}^2$



Example: $R \sim 1 \mu\text{m}$

$V_{\text{max}} \sim 10 \mu\text{m}/\text{sec}$
 $\mu \sim 10^{-3} \text{ kg/m}\cdot\text{s}$

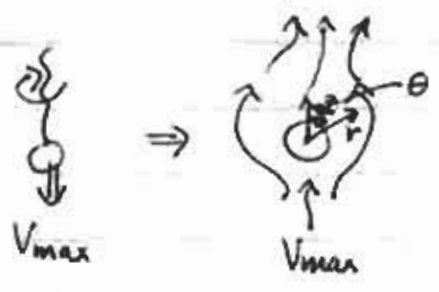
$F_{\text{drag}} \sim 200 \text{ pN}$

$\sim 10^4 - 10^5$ adhesion receptor (ECM bonds per cell ($10^3 \text{ pN}/\text{cell}$)
 each $\sim 1 \text{ pN}$

cell $\sim 10 \mu\text{m}$ radius $\Rightarrow \sim 100 \mu\text{m}^2$ surface area

Stopping distance?
 $m_a = 6\pi \mu V_{\text{max}} R$
 $V_{\text{max}} = 0.10^2 \mu\text{m}$

Example #2:



Stoke's Eqn

$$0 = \nabla p + \mu \nabla^2 \mathbf{v}$$

Viscous drag force

$$\tau_{\theta r}(R, \theta) = -\frac{3}{2} \mu V_{\text{max}} \sin \theta$$

Pressure force: $p(r, \theta) = -\frac{3}{4} \frac{\mu V_{\text{max}} (R/r)^2 \cos \theta}{R}$

B.C. $r \rightarrow \infty, \text{all } \theta, v(r, \theta) \rightarrow V_{\text{max}}$
 $r \rightarrow \infty, \text{all } \theta, p \rightarrow p_{\infty}$

See example 7.4-2 Deen text: $v_r(r, \theta) = V_{\text{max}} \cos \theta \left[1 - \frac{3}{2} \left(\frac{R}{r}\right) + \frac{1}{2} \left(\frac{R}{r}\right)^3 \right]$

Overall force: $F = -2\pi R^2 \int_0^\pi [p(R, \theta) \cos \theta + \tau_{\theta r}(R, \theta) \sin \theta] d\theta$